



Distributed Microphone Array Signal Processing for Hearing Aids

Prof. Dr. Simon Doclo Signal Processing Group, University of Oldenburg

> simon.doclo@uni-oldenburg.de http://www.sigproc.uni-oldenburg.de

Outline

- Hearing instruments: bilateral vs. binaural processing

 Information exchange using wireless link
- Binaural noise reduction techniques
 - o Objective: noise reduction and binaural cue preservation
 - o Binaural beamforming, CASA, Multi-channel Wiener filter
 - o Experimental results
- Bandwidth reduction: transmit only one contralateral signal
 o iterative distributed MWF → converges to binaural MWF
- Effect of capacity of wireless link on performance
- Extension to acoustic sensor networks

Hearing impairment

- Hearing aids
 -Problems
 - -Bilateral binaural
- Binaural processing
- Bandwidth reduction
- Acoustic sensor networks
- Conclusion

- Hearing impairment effects about 15% of population
- Sensorineural hearing loss: damage to the hair cells in the cochlea
 - \rightarrow Increased hearing threshold
 - \rightarrow Reduced dynamic range
 - \rightarrow Reduced frequency selectivity

Understanding speech in background noise = very difficult!

- Severity of hearing loss
 - o Mild to severe \rightarrow hearing aid
 - o Profound hearing loss / deafness \rightarrow cochlear implant



Hearing instruments

- Hearing aids
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- Possibilities with analog hearing aids = limited!
- **Developments** in HW and micro-electronics:
 - o Digital signal processor
 - o Multiple microphones (2-3)
 - o Binaural wireless link between hearing aids
- Digital hearing instruments and cochlear implants allow for advanced acoustical signal (pre-)processing
- Important algorithmic constraints:
 - o Input-output latency (< 10...15 ms)
 - o Power constraints from small battery







Hearing instruments

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- Basic processing: acoustic amplification and dynamic range compression (frequency-selective)
- Due to acoustic coupling between receiver and microphone (large amplification): acoustic feedback control
- Increase speech intelligibility in background noise: single- or multi-microphone noise reduction and dereverberation



Hearing instruments

• Major problems: background noise, directional hearing

- o signal processing to selectively enhance useful speech signal and improve speech intelligibility
- o signal processing to preserve directional hearing (binaural auditory cues) and spatial awareness
- o robustness important due to small inter-microphone distance

Binaural auditory cues

- o Interaural Time Difference (ITD) Interaural Level Difference (ILD)
- o Binaural cues, in addition to spectral and temporal cues, play an important role in binaural noise reduction and sound localisation
- o ITD: f < 1500Hz, ILD: f > 2000Hz



Hearing aids -Problems

- -Bilateral binaural
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Bilateral vs. Binaural

Bilateral system Hearing aid user $Y_{1,0}(\omega)\cdots Y_{1,M_1-1}(\omega)$ $Y_{0,0}(\omega)\cdots Y_{0,M_0-1}(\omega)$ $\mathbf{W}_0(\omega)$ $W_1(\omega)$ $Z_0(\omega)$ $Z_1(\omega)$

Hearing aid user $Y_{1,0}(\omega)\cdots Y_{1,M_1-1}(\omega)$ $Y_{0,0}(\omega)\cdots Y_{0,M_0-1}(\omega)$ $W_1(\omega)$ $\mathbf{W}_0(\omega)$ $Z_0(\omega)$ $Z_1(\omega)$

Binaural system

Independent left/right processing: Preservation of binaural cues for localisation ?

- Hore microphones:
 - \rightarrow better performance ?
 - \rightarrow preservation of binaural cues ?
- Θ

Hearing aids Problems Bilateral - binaural

- Binaural processing
- Bandwidth reduction
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- Conclusion

Bilateral vs. Binaural

Bilateral system:

- o Independent processing of left and right hearing aid
- o Negative effect on localisation cues and intelligibility through binaural hearing advantage [Van den Bogaert et al., 2006]





FIG. 5. Mean speech reception thresholds obtained in experiment I for three different noise types : FF (free field), dL (headshadow only), and dT (ITD only). The closed data points represent results of Plomp and Mimpen (1981) obtained in a free field.

[Bronkhorst and Plomp, 1988]

[Beutelmann and Brand, 2006] 8

Hearing aids -Problems

-Bilateral - binaural

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- Binaural processing
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Bilateral vs. Binaural

Bilateral system

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- o Independent processing of left and right hearing aid
- o Negative effect on localisation cues and intelligibility through binaural hearing advantage [Van den Bogaert et al., 2006]

Binaural system

- o Cooperation between left and right hearing aid (e.g. wireless link) \rightarrow centralised vs. distributed processing
- o Bandwidth constraint and latency of wireless link

Objectives/requirements for binaural algorithm:

- 1. SNR improvement: noise reduction, limit speech distortion
- 2. Preservation of binaural cues (all sources) to exploit binaural hearing advantage
- 3. No assumption about position of speech source and microphones

Hearing aids -Problems

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Binaural noise reduction techniques

- Hearing aids
- Binaural processing
- -Algorithms
- -Binaural MWF
- -Experiments
- Bandwidth reduction
- Acoustic sensor networks
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• Configuration: microphone array with *M* microphones at left and right hearing aid, communication between hearing aids

$$X_{0,m}(\omega) = X_{0,m}(\omega) + V_{0,m}(\omega), \quad m = 0...M_0 - 1$$
speech coordspondent

- Vector notation: $\mathbf{Y}(\omega) = \mathbf{X}(\omega) + \mathbf{V}(\omega)$
- One desired signal source: $\mathbf{X}(\omega) = \mathbf{A}(\omega)S(\omega)$
 - $A(\omega)$ = transfer function (TF) vector between source and mic array



Binaural noise reduction techniques

Hearing aids

Binaural processing

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- -Algorithms
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Use microphone signals to compute output signal at both ears \rightarrow computation of filters W_0 and W_1

$$Z_0(\omega) = \mathbf{W}_0^H(\omega)\mathbf{Y}(\omega), \quad Z_1(\omega) = \mathbf{W}_1^H(\omega)\mathbf{Y}(\omega)$$

$$\mathbf{W}(\boldsymbol{\omega}) = \begin{bmatrix} \mathbf{W}_0(\boldsymbol{\omega}) \\ \mathbf{W}_1(\boldsymbol{\omega}) \end{bmatrix}$$



Hearing aids

Binaural processing
 Algorithms

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- -Binaural MWF -Experiments
- Bandwidth reduction
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Binaural noise reduction techniques

- Fixed beamforming: spatial selectivity + binaural speech cues
 - o Maximize directivity index while restricting speech ITD error [Desloge, 1997]
 - o Superdirective beamformer using HRTFs [Lotter, 2004]
 - ➔ low computational complexity
 - Ilimited performance, known geometry, only speech cues may be preserved (in ideal situations)



[Desloge, 1997]

Binaural noise reduction techniques

- Hearing aids
- Binaural processing
 Algorithms

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- Adaptive beamforming: based on GSC-structure
 - Divide frequency spectrum: low-pass portion unaltered to preserve ITD cues, high-pass portion processed using GSC
 - preserves binaural cues to some extent
 - Substantial drop in noise reduction performance, known geometry



[Welker, 1997]

Hearing aids

Binaural processing
 Algorithms

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Binaural noise reduction techniques

- CASA-based techniques [Kollmeier, Lotter, Rohdenburg, Wittkop]
 - o Computation and application of **real-valued** binaural mask based on binaural and temporal/spectral cues
 - o Can be merged with MVDR-beamformer or ICA-based processing
 - Good preservation of binaural cues for **all** sources

"single-microphone spectral enhancement" artefacts at low SNRs





[Reindl 2010, Saruwatari 2010]

Binaural noise reduction techniques

Hearing aids

Binaural processing
 -Algorithms
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[S. Doclo, S. Gannot, M. Moonen, A. Spriet, Handbook on Array Processing and Sensor Networks, Wiley, 2010.]

[S. Doclo, T.J. Klasen, M. Moonen, T. Van den Bogaert, J. Wouters, R.P. Derleth, S. Korl, US2010002886.]

- Binaural multi-channel Wiener filter [Doclo, Van den Bogaert, Moonen]
 - o MMSE estimate of speech component in microphone signal at both ears



noise cues may be distorted

Extension of MWF:

preservation of binaural speech and noise cues without substantially compromising noise reduction performance

Binaural MWF

- Hearing aids
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Binaural multi-channel Wiener filter: estimate of speech
 component in microphone signal at both ears (usually front mic)
 + trade-off between noise reduction and speech distortion

$$\mathbf{r}(\mathbf{W}) = E \left\{ \begin{bmatrix} \mathbf{X}_{0,r_0} & \mathbf{W}_0^H \mathbf{X} \\ \mathbf{X}_{1,r_1} & \mathbf{W}_1^H \mathbf{X} \end{bmatrix}^2 + \mu \begin{bmatrix} \mathbf{W}_0^H \mathbf{V} \\ \mathbf{W}_1^H \mathbf{V} \end{bmatrix}^2 \right\} \implies \mathbf{W}_{SDW} = \mathbf{R}^{-1} \mathbf{r}$$

speech component
in from the photon noise reduction
$$\mathbf{R} = \begin{bmatrix} \mathbf{R}_x + \mu \mathbf{R}_v & \mathbf{0}_M \\ \mathbf{0}_M & \mathbf{R}_x + \mu \mathbf{R}_v \end{bmatrix}, \quad \mathbf{r} = \begin{bmatrix} \mathbf{r}_{x0} \\ \mathbf{r}_{x1} \end{bmatrix}, \quad \mathbf{R}_x = \mathbf{R}_y - \mathbf{R}_y$$

- o Estimate \mathbf{R}_{y} during speech-dominated time-frequency segments, estimate \mathbf{R}_{v} during noise-dominated segments, requiring robust voice activity detection (VAD) mechanism
- o No assumptions about positions of microphones and sources
- o Low-cost real-time implementation using multi-channel frequency-domain criterion and stochastic gradient algorithm

Binaural MWF

- Hearing aids
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Interpretation for a single speech source

o Spectral and spatial filtering operation

$$\mathbf{W}_{SDW,0} = \underbrace{\mathbf{\Gamma}_{v}^{-1}\mathbf{A}}_{\mathbf{A}^{H}\mathbf{\Gamma}_{v}^{-1}\mathbf{A}} \cdot \underbrace{\mathbf{A}^{H}\mathbf{\Gamma}_{v}^{-1}\mathbf{A}}_{\mathbf{A}^{H}\mathbf{\Gamma}_{v}^{-1}\mathbf{A} + \underbrace{\mu P_{v} / P_{s}}_{\mathbf{A}^{*}} A_{0,r_{0}}^{*}$$

Spatial separation between speech and noise sources

SNR

- with Γ (spatial) coherence matrix and P (spectral) power
- o SNR improvement

$$\text{SNR}_L^{\text{out}} = \text{SNR}_R^{\text{out}} = \rho = P_s \mathbf{A}^H \mathbf{R}_v^{-1} \mathbf{A}.$$

o Binaural cues (ITD – ILD)

$$\mathbf{W}_{SDW,0} = \mathrm{ITF}_{x,in}^* \mathbf{W}_{SDW,1}$$

 Hearing aids

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[B. Cornelis, S. Doclo, T. Van den Bogaert, J. Wouters, M. Moonen, IEEE Trans. Audio, Speech and Language Processing, Feb. 2010.]

Partial noise estimation (MWFv)

Partial estimation of noise component

o Estimate of sum of speech component and scaled noise component

$$J(\mathbf{W}) = E\left\{ \left\| \begin{bmatrix} X_{0,r_0} - \mathbf{W}_0^H \mathbf{X} \\ X_{1,r_1} - \mathbf{W}_1^H \mathbf{X} \end{bmatrix} \right\|^2 + \mu \left\| \begin{bmatrix} \eta V_{0,r_0} - \mathbf{W}_0^H \mathbf{V} \\ \eta V_{1,r_1} - \mathbf{W}_1^H \mathbf{V} \end{bmatrix} \right\|^2 \right\}, \quad 0 \le \eta \le 1$$

o Relationship with SDW-MWF: mix with reference microphone signals

$$Z_0 = \eta Y_{0,r_0} + (1 - \eta) Z_{SDW,0}$$
$$Z_1 = \eta Y_{1,r_1} + (1 - \eta) Z_{SDW,1}$$

> reduction of noise reduction, but not necessarily of intelligibility

$$\Delta SNR_L = \Delta SNR_L^o \frac{\left(\frac{\eta\mu+\rho}{\mu+\rho}\right)^2}{\left(\frac{\eta\mu+\rho}{\mu+\rho}\right)^2 + (\Delta SNR_L^o - 1)\eta^2}$$



works for multiple noise sources

Interaural Wiener filter (MWF-ITF)

Hearing aids

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[B. Cornelis, S. Doclo, T. Van den Bogaert, J. Wouters, M. Moonen, IEEE Trans. Audio, Speech and Language Processing, Feb. 2010.]

Extension of SDW-MWF with binaural cues

- o Add term related to binaural cues of noise (and speech) component
- o Possible cues: ITD, ILD, Interaural Transfer Function (ITF)

e.g.
$$ITF_{in}^{\nu} = \frac{V_{0,r_0}}{V_{1,r_1}} = \frac{E\left\{V_{0,r_0}V_{1,r_1}^*\right\}}{E\left\{V_{1,r_1}V_{1,r_1}^*\right\}} \qquad ITF_{out}^{\nu} = \frac{Z_{\nu 0}}{Z_{\nu 1}} = \frac{\mathbf{W}_0^H \mathbf{V}}{\mathbf{W}_1^H \mathbf{V}}$$

$$f_{t}(\mathbf{W}) = E \left\{ \left\| \begin{bmatrix} X_{0,r_{0}} - \mathbf{W}_{0}^{H} \mathbf{X} \\ X_{1,r_{1}} - \mathbf{W}_{1}^{H} \mathbf{X} \end{bmatrix} \right\|^{2} + \mu \left\| \begin{bmatrix} \mathbf{W}_{0}^{H} \mathbf{V} \\ \mathbf{W}_{1}^{H} \mathbf{V} \end{bmatrix} \right\|^{2} \right\}$$

$$+ \alpha E \left\{ \left\| \mathbf{W}_{0}^{H} \mathbf{X} - ITF_{in}^{x} \mathbf{W}_{1}^{H} \mathbf{X} \right\|^{2} \right\} + \beta E \left\{ \left\| \mathbf{W}_{0}^{H} \mathbf{V} - ITF_{in}^{y} \mathbf{W}_{1}^{H} \mathbf{V} \right\|^{2} \right\}$$

ITF preservation speech

ITF preservation noise

Closed form expression

Although output ITF of speech and noise component is equal,

output ITF depends on output SNR \rightarrow positive perceptual effect

$$ITF^{out} = \frac{ITF_x^{in} - \xi(ITF_x^{in} - ITF_v^{des})}{1 + \xi ITF_v^{des,*}(ITF_x^{in} - ITF_v^{des})}$$



(†

 J_{to}

Implicit assumption of single noise source, difficult parameter tuning

Experimental results

Identification of HRTFs

- o Binaural recordings on CORTEX MK2 artificial head
- o 2 omni-directional microphones on each hearing aid (d=1cm)
- o $LS = -90^{\circ}:15^{\circ}:90^{\circ}, 90^{\circ}:30^{\circ}:270^{\circ}, 1m$ from head
- o Conditions: T_{60} =510 ms, f_s =16 kHz

<image>

Hearing aids

Binaural processing
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 Binaural MWF

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Hearing aids

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- -Binaural MWF
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vol. 124, no. 1, Jul. 2008.]

Conclusion

Perceptual evaluation: MWFv

- SRT measurements (headphone presentation, 10 normal-hearing) •
- Speech sentences + babble noise •
- Algorithms: state-of-the art bilateral (ADM), MWF, MWFv (η =0.2) •
- Conditions: S_0N_{60} , $S_{90}N_{270}$ and $S_0N_{90/180/270}$ ٠

	$S_0 N_{60}$			$S_{90}N_{270}$			S ₀ N _{90/180/270}		
Bilat/bin Δ SRT (dB)	Perceptual	Left	Right	Perceptual	Left	Right	Perceptual	Left	Right
ADM	2.1 ± 1.9	2.7	2.8	$-4.3 \pm 1.3^{*}$	4.3	-3.2	1.3 ± 1.4	6.0	5.9
MWF ₂₊₂	$4.3 \pm 1.5*$	4.9	9.6	0.7 ± 1.4	10.0	2.5	$4.6 \pm 0.8 *$	7.1	7.2
MWF ₂₊₁	$3.8 \pm 1.6^{*}$	4.0	6.2	0.3 ± 2.0	9.6	2.1	$4.0 \pm 1.5^{*}$	6.6	6.0
MWF ₂₊₀	$1.0 \pm 0.7 *$	1.9	3.3	-1.2 ± 1.6	3.8	1.0	$2.8 \pm 1.3^{*}$	5.1	4.9
MWF ₂₊₂ -N _{0.2}	$3.6 \pm 1.4^*$	3.3	5.4	$2.0 \pm 1.4^{*}$	4.3	1.9	$3.2 \pm 0.8*$	4.1	4.2
MWF ₂₊₁ -N _{0.2}	$2.7 \pm 1.3*$	2.6	3.0	1.5 ± 1.6	3.9	1.6	$3.4 \pm 0.8*$	3.7	3.3
MWF ₂₊₀ -N _{0.2}	1.0 ± 2.1	1.1	0.9	0.0 ± 1.5	1.0	0.7	$2.3 \pm 1.4^{*}$	2.8	2.6
[T. Van den Bogaert, S.									
Moonen, Journal of the Acoustical Society of America,									21

Perceptual evaluation: MWFv

- Algorithms: unprocessed, state-of-the art bilateral, MWF, MWFv (η=0.2)
- Conditions: S_0N_{60} , $S_{45}N_{315}$ and $S_{90}N_{270}$



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Hearing aids

- Binaural processing
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[T. Van den Bogaert, S. Doclo, J. Wouters, M. Moonen, Journal of the Acoustical Society of America, Jan. 2009.]

Audio demo

Speech and noise material:

o HINT sentences, speech source in front (0°)

- o Multi-talker babble noise at 60°
- o SNR=0 dB, f_s =16 kHz, FFT-size N=256, μ =1, α =0

	Noisy	Speech	Noise
Input		And the second s	A
Output (β=0)	₩		₩
Output (β=0.05)	A		A

Hearing aids

Binaural processing
 -Algorithms

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Binaural processing

- Remaining challenges
 - o Algorithm exploiting information in **all** microphones, preserving binaural cues for **all** sources
 - o Psycho-acoustics: how much **distortion of binaural cues** can be tolerated
 - \rightarrow related to good **objective measures**

- Hearing aids
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• Binaural MWF

- o **all** microphone signals are transmitted over wireless link
- Reduce bandwidth requirement of wireless link by transmitting one signal from contralateral ear
 - o Raw microphone signal (e.g. front)
 - o Output of fixed (e.g. superdirective) beamformer
 - o MWF-estimate using only contralateral microphone signals
 - o Iterative distributed binaural MWF scheme (DB-MWF)



- Hearing aids
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 Distributed MWF
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[S. Doclo, T. Van den Bogaert, M. Moonen, J. Wouters, IEEE Trans. Audio, Speech and Language Processing, Jan. 2009.]

• Iterative procedure

- Hearing aids
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o In each iteration \mathbf{F}_{10} is equal to \mathbf{W}_{00} from previous iteration, and \mathbf{F}_{01} is equal to \mathbf{W}_{11} from previous iteration



Single speech source

- Hearing aids
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o MWF cost function decreases in each step of iteration

$$J\left(\left[\begin{array}{c} \mathbf{W}_{0}^{i+1} \\ \mathbf{W}_{1}^{i+1} \end{array}\right]\right) \leq J\left(\left[\begin{array}{c} \mathbf{W}_{0}^{i} \\ \mathbf{W}_{1}^{i} \end{array}\right]\right)$$

o Remarkably: convergence to B-MWF solution (!)

$$\mathbf{W}_0^\infty = \mathbf{W}_0^m, \quad \mathbf{W}_1^\infty = \mathbf{W}_1^m$$

- General case where **R**_x is not a rank-1 matrix
 - o MWF cost function does not necessarily decrease in each iteration
 - o usually no convergence to optimal B-MWF solution
 - o Although $J_0(\mathbf{W}_0^{\infty}) \ge J_0(\mathbf{W}_0^m)$, $J_1(\mathbf{W}_1^{\infty}) \ge J_1(\mathbf{W}_1^m)$, DB-MWF procedure can be used in practice and approaches binaural MWF performance
- Procedure can be extended to
 - o Multiple sensor arrays and multiple desired sources [Bertrand 2010]
 - o Binaural MVDR-beamformer [Golan 2010]



- Hearing aids
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Contralateral directivity patterns



- Hearing aids
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Investigate effect of capacity of binaural link \rightarrow encode signal(s) at finite bit-rate *R* before transmission to contralateral side



- PRate-distortion: $R(\lambda) = \frac{1}{4\pi} \int_{-\infty}^{\infty} \max\left(0, \log_2 \frac{\Phi_Y^{01}(\omega)}{\lambda}\right) d\omega$ PSD of transmitted signal $V_{01}(\omega)$
- Upper bound on achievable performance can be calculated using forward channel representation



$$B = \max\left(0, \frac{\Phi_Y^{01} - \lambda}{\Phi_Y^{01}}\right)$$

$$\Phi_W = \max\left(0, \lambda \frac{\Phi_Y^{01} - \lambda}{\Phi_Y^{01}}\right)$$

- Hearing aids
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- Investigate effect of rate constraints on performance of binaural MWF and distributed MWF
- Setup and performance measures:
 - o Binaural hearing aid configuration (M=2, d=1cm)
 - o Speech source at 0°, interference at 330°, uncorrelated noise

 $\boldsymbol{\Phi}_{y} = \boldsymbol{\Phi}_{s} \mathbf{A}_{s} \mathbf{A}_{s}^{H} + \boldsymbol{\Phi}_{i} \mathbf{A}_{i} \mathbf{A}_{i}^{H} + \boldsymbol{\Phi}_{u} \mathbf{I}_{2M}$

- Involved PSDs are assumed to be flat (8 kHz), SIR=0 dB, SNR=20 dB
- ATFs modelled using spherical head shadow model, no reverberation
- o MWF-based algorithms: $\mu = 1$
- **Performance measure**: ratio between MSE at rate 0 and MSE at rate *R*, *i.e.* effect of availability of binaural link

$$G(R) = 10\log_{10}\frac{\xi(0)}{\xi(R)}$$

ps. only performance at left hearing aid is shown

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- Effect on performance of binaural MWF
 - o Total link capacity *R* distributed between front/back microphone

 $R_f = (1 - \rho)R, \quad R_b = \rho R$



For low bit-rate highest performance when transmitting single mic, from certain bit-rate beneficial transmitting both mics

- Hearing aids
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- Effect on performance of distributed MWF
 - o Single signal is compressed/transmitted in each iteration
 - o Case 1: total capacity *R* evenly distributed between iterations



- For infinite rate, DB-MWF converges to B-MWF
- More iterations only improve performance at high rates

- Hearing aids
- Binaural processing

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- Effect on performance of distributed MWF
 - o Single signal is compressed/transmitted in each iteration
 - o Case 2: spread iterations over subsequent frames (stationarity)



DB-MWF scheme converges after K=2 iterations, moreover achieving highest performance gain

Binaural processing

Remaining challenges

o Algorithm exploiting information in **all** microphones, preserving binaural cues for **all** sources

o Psycho-acoustics: how much **distortion of binaural cues** can be tolerated

- \rightarrow related to good **objective measures**
- o (Perceptual) coding of transmitted signal

o Technical issues of wireless link:

- Latency requirements
- Synchronisation between both hearing aids

Hearing aids

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Extension to more mic arrays...

Ad-hoc acoustic sensor networks

- Network of tens of small, low-power microphones with wireless communication capability → improvement in performance and flexibility (ambient intelligence)
- o **Objectives:** speech enhancement and source localisation

o Prototype applications:

- Hearing aids using extra microphones (room, mobile phones, ...)
- Video-conferencing using all microphones on laptops / room

0 Challenges:

- Dynamic array configuration: large number of microphones at unknown positions, dynamically select subset of microphones
- Distributed and collaborative algorithms
- Synchronisation issues
- Useful in other, e.g.
 biomedical and digital
 communication, applications
 (body area network)



Conclusions

- Hearing aids
- Binaural processing

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- Bandwidth reduction
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- Signal processing in binaural hearing instruments
 - o Objective: noise reduction and preservation of binaural cues
 - o Information exchange and collaboration through wireless link
 - o Algorithms: beamforming, CASA, MWF
- Bandwidth reduction by transmitting filtered combination of contralateral microphone signals
 - o Raw microphone signal, contralateral MWF estimate
 - DB-MWF: iterative procedure, which converges to B-MWF
 for rank-1 speech correlation matrix
- Effect of bit-rate on performance using rate-distortion theory
 - o DB-MWF achieves highest performance gain, when iterations can be spread over subsequent frames
- Extension: distributed processing in acoustic sensor networks
 - o Challenges: dynamic array configuration, collaborative algorithms
 - o Mounting interest: half of papers in best student session!

Questions ?



House of Hearing, Oldenburg