

Acoustically Transparent Hearing Device: Towards Integration of Individualized Sound Equalization, Electro-Acoustic Modeling and Feedback Cancellation

Florian Denk¹, Steffen Vogl², Henning Schepker¹, Birger Kollmeier¹, Matthias Blau², <u>Simon Doclo¹</u>

¹ Dept. of Medical Physics and Acoustics and Cluster of Excellence "Hearing4All", University of Oldenburg, Germany

² Institut für Hörtechnik und Audiologie, Jade Hochschule Oldenburg







Motivation: *HiFi* Hearing Device

- Current hearing devices: sound quality still limited (e.g., distortion, non-individualized, own voice, spatial impression)
- Aim: construct a *scalable hearing device*
 - Acoustically Transparent: no degradation of perceived sound environment in "ground state"
 - Possibility to provide hearing support (e.g., amplification, DRC, noise reduction) when required









- Custom in-the-ear earpiece with relatively open acoustics
- Vent/core: 2 microphones and 2 receivers (woofer/tweeter)
- Concha: 1 microphone

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 Electronics interchangeable, insertion into individual silicone ear mould or generic earplugs









[Denk et al., International Journal of Audiology, 2017]





Transparent Hearing System

1. Transparent sound presentation:

 Natural sound quality by equalizing to open-ear target response at eardrum

2. Individualized Electro-Acoustic Model:

- Better understand acoustics
- Predict sound pressure and transfer functions (eardrum)



3. Acoustic Feedback cancellation

 Exploit multiple microphones to steer null towards position of receiver

- 4. Hearing support:
- Amplification and dynamic range compression
- Noise reduction (active/passive)
- Occlusion
 management







1. Transparent sound presentation

- Target pressure at eardrum = pressure that is (physically or perceptually) equal to pressure with open ear, i.e. individual head-related transfer function (HRTF)
 - Estimate target pressure based on outer microphone(s), e.g., frequency-dependent gain T
 - 2. Equalization with hearing device: adjust filter G(k) such that direct sound + device output = target
- In-Situ calibration routine, assuming that pressure at in-ear microphone and eardrum are similar

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1. Transparent sound presentation

- Perceptual sound quality evaluation (NH subjects):
 - Transparency mode almost indistinguishable from (simulated) open ear canal condition, also in combination with HA processing
 - Significantly outperforms behind-the-ear (BTE)







1. Transparent sound presentation

• Physical Evaluation:

- Real-ear measurements on 12 subjects
- Real Ear Insertion Gain (REIG):0 dB for transparency

Potential error sources:

- Estimation of target response
- Calibration: estimation of pressure at the eardrum ≠ inner-ear mic







2. Electro-acoustic model

- Earpiece Model (Fixed)





2. Electro-acoustic model

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Parameter optimization (4 radii, 1 length, 1 resistive load) by minimizing the difference between measured and modeled ear canal (Nelder-Mead simplex optimization procedure):

$$J(p) = \sum_{\substack{f_{\text{valid}}\\ \text{ossietzxy}\\ \text{ossietzxy}\\ \text{ossietzxy}}} (db(Z_{ec,\text{meas}}) - db(Z_{ec,\text{model}}(p)))^2 + 10 \cdot (arg(Z_{ec,\text{meas}}) - arg(Z_{ec,\text{model}}(p)))^2$$



2. Electro-acoustic model

- Evaluation (sound pressure at ear drum) for 12 subjects

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accurate prediction of sound pressure at ear drum using individualized electro-acoustic model up to about 6 kHz





3. Acoustic feedback cancellation

- Several approaches for acoustic feedback cancellation in hearing aids:
 - 1. Feedforward suppression
 - 2. Adaptive feedback cancellation (prediction error method, probe noise)
 - 3. Spatial filtering methods exploiting multiple microphones
- Approach: fixed beamformer steering spatial null towards position of hearing aid receiver → theoretically perfect feedback cancellation possible
- Extension: reduction of residual feedback using adaptive filter









3. Acoustic feedback cancellation

- Assumptions:
 - Time-invariance of the acoustic feedback paths
 - Availability of multiple (measured) acoustic feedback paths
- Different optimization criteria: compute coefficients b of null-steering beamformer by minimizing cost function (least-squares, minimax)
- Increase robustness by including all available feedback paths H_i, i=1...I

$$\frac{\min_{\mathbf{b}} \quad J(\mathbf{b})}{\text{subject to} \quad B_{m_0}(q) = q^{-L_d}} \qquad J_{rLS}(\mathbf{b}) = \sum_{i=1}^{l} \sum_{n=0}^{N_{FFT}-1} |\mathbf{H}_i^H(\omega_n)\mathbf{B}(\omega_n)|^2 \\ J_{rMM}(\mathbf{b}) = \max_{\omega_n, i=1, \dots, l} |\mathbf{B}^H(\omega_n)\mathbf{H}_i(\omega_n)|^2$$

 Note: directional response of beamformer for external signals is not explicitly constrained/optimized





3. Acoustic feedback cancellation

- Feedback cancellation performance [Schepker et al., ITG2016]
- **Directional response of beamformer** (relative to entrance microphone)



(robust) average ASG improvement of more than 20 dB

 $20 \log_{10} |\tilde{D}(f,\theta_j)/D_2(f,\theta_j)| \; [\mathrm{dB}]$ 2 f=250 Hz f=500 Hz f=1000 H -6 f=2000 H =f=4000 Hz f=8000 Hz -8 -180 -120-60 0 60 120180 Incident angle θ [°]

small variations in directional response of approximately ± 4dB



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Conclusion and outlook

Acoustically transparent hearing device:

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- Earpiece with multiple integrated microphones and receivers
- Allows for individualized sound pressure equalization and beamforming for acoustic feedback cancellation
 - Transparency mode almost indistinguishable from open ear canal
 - Robust ASG improvement of more than 20 dB
- Real-time demonstrator available

Outlook:

- Integration of individualized electro-acoustic model into equalization procedure
- Combined solutions for equalization and acoustic feedback cancellation (exploting multiple receivers)
- Integration with hearing support (e.g., noise suppression) and occlusion management

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